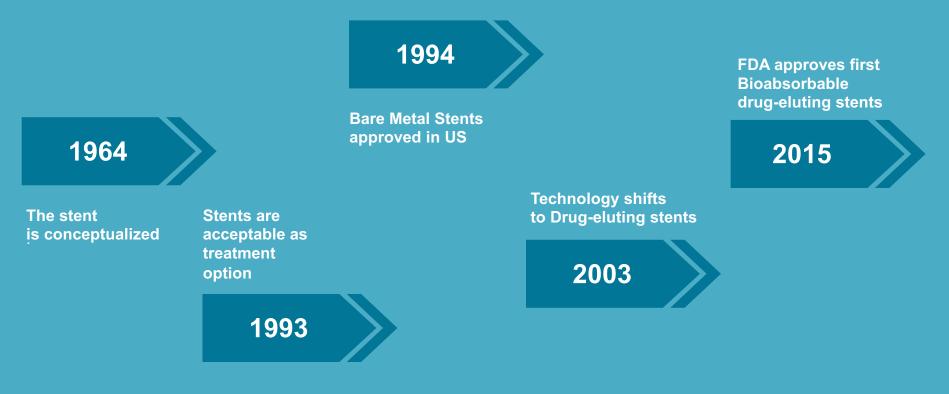
Historical milestones in coronary stents



[1] Tomberli B et al., A Brief History of Coronary Artery Stents, Rev Esp Cardiol (Engl Ed). 2018 May;71(5):312-319.



Stent market



150 million

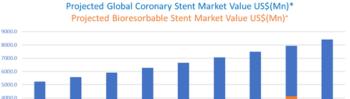
The global bioresorbable Coronary stents market size is estimated currently at 150 million

2023

2024



2000.0



Total Market

Bioresobable Vascular Scaffolds

Bioresorbable Stent Market CAGR 8.5%

MARKET PLAYER Boston Scientific, Biotronik, Elixir Medical Corporation,

Johnson and Johnson, REVA

[1] Coronary Stents: Market Size, Share and Global Trend By Deployment (Self and Balloon-expandable), Stent Type (Drug Eluting Stent, Bioresorbable Stent, Bare Metal Stent, Covered Stent and Others), End User (Hospitals, Ambulatory Surgical Centers, Specialty Clinics, Catheterization Labs) and Geography Forecast till 2025. Fortune Business Insights; May 2019 [2] Bioabsorbable Stents Market - Growth, Trends, and Forecast (2019 - 2024). Research and Markets; February 2019

How it works?



Absorb Bioabsorbable drug-eluting stent

Absorb Stent



The scaffold is inserted into the artery on a balloon at the end of a thin flexible tube

The scaffold is expanded by inflating the balloon, pushing the plaque against the artery to enable blood flow The balloon is removed, leaving the scaffold to slowly release medication to the diseased area

Blood flow is restored and the scaffold begins dissolving Over time, the scaffold dissolves into the blood vessel, which remains open without support



Pre-clinical testing and clinical studies

Preclinical testing (*in vitro* and *in vivo*) includes the testing of materials and stents before being tested in humans.

Clinical studies



Stent design (length, strut thickness, diameter, etc)

Patient-specific characteristics (gender, diabetes)

Type of drug

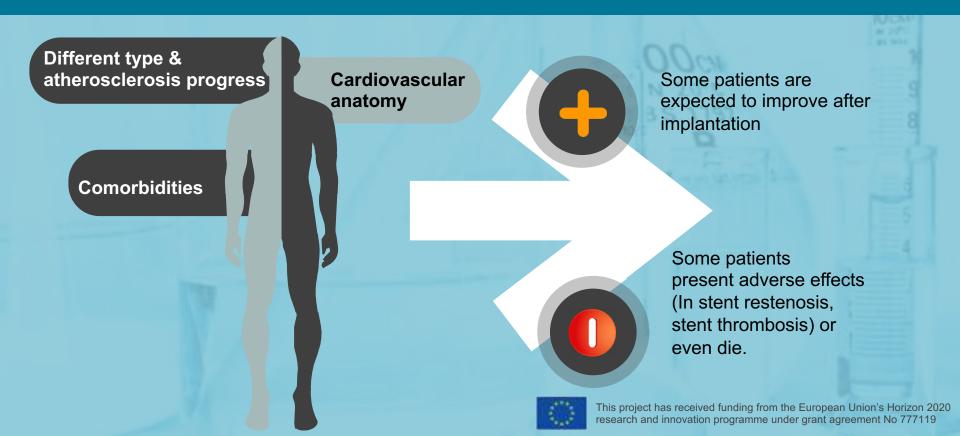
Type of vessel (long lesions, number of stenosis, plaque composition)

Type of biodegradable polymer

Stenting technique (two versus one stent)

Limitations of clinical studies





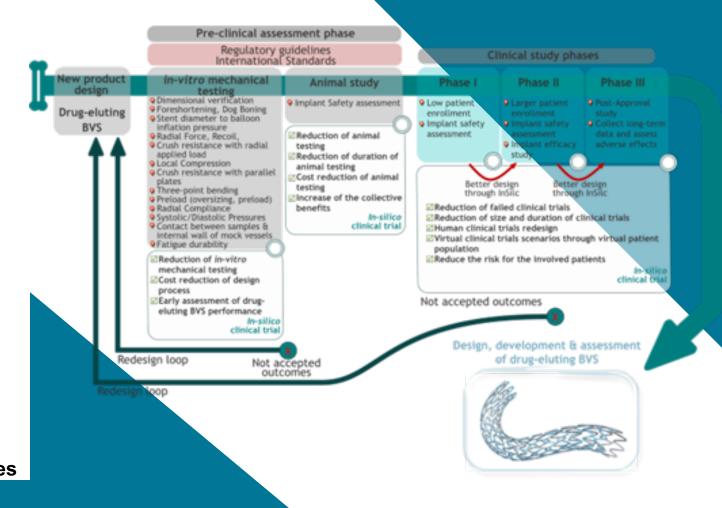
- Percutaneous coronary intervention with stents is the most widely performed procedure for symptomatic coronary disease treatment
- Despite major developments , in stent restenosis remains between 5 -10%.
- These long-term limitations of conventional stents may be overcome to a degree by using drug-eluting BVS.

WHY InSilc?



[1] Pan et al., Interv Cardiol. 2019 Feb;14(1):10-16. doi: 10.15420/icr.2018.39.1.

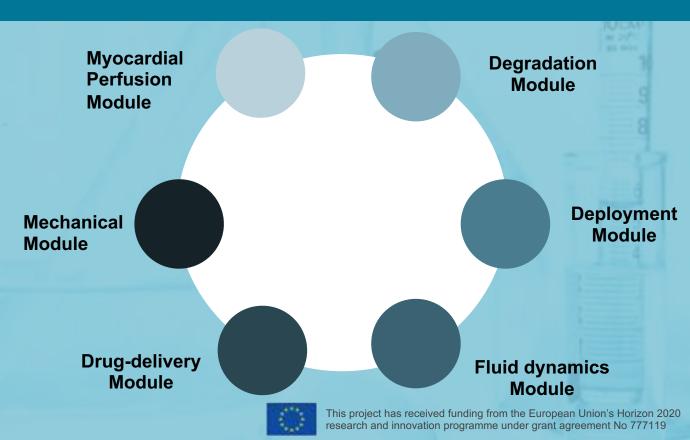
InSilc develops an in-silico clinical trial (ISCT) **platform** for designing, developing and assessing drugeluting bioresorbable vascular scaffolds (BVS), by building on the comprehensive **biological** & biomedical knowledge and advanced modelling approaches

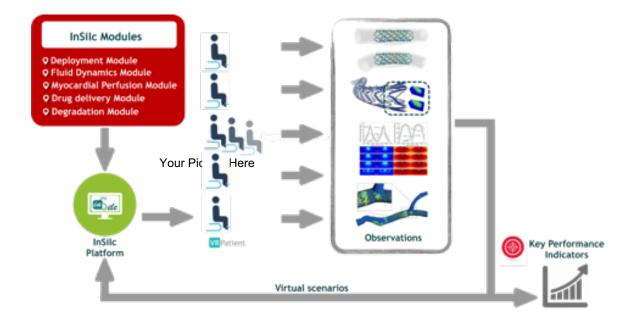


Overall concept



InSilc platform is based on the extension of existing multidisciplinary and multiscale models that simulate the drug-eluting BVS performance



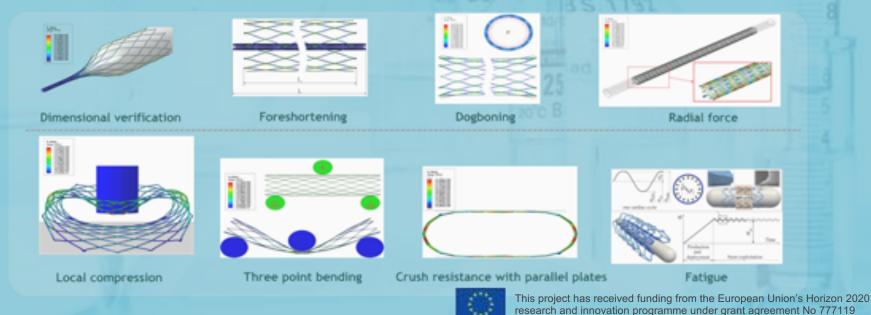


InSilc Modules

Mechanical modelling Module



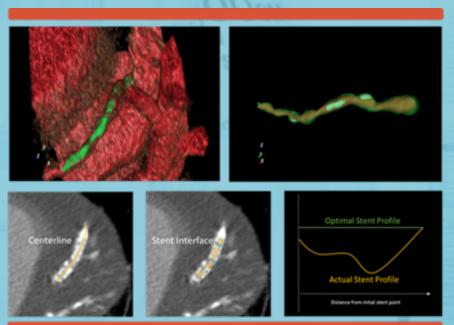
 Replace all the mechanical *in vitro* tests required for the BVS by technical standard:



3D Reconstruction and plaque characterisation tool



- The 3D Reconstruction and plaque characterisation tool incorporates a state of the art method for 3D arterial tree reconstruction based on level set methods developed in SMARTool project.
- The method is able to accurately reconstruct the arterial tree including lumen, outer wall, calcified and noncalcified plaques.

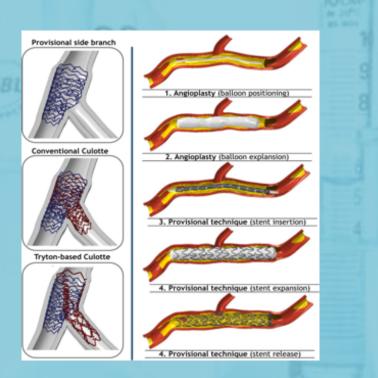




Deployment Module



- "Virtual" deployment in single stenosed or bifurcated coronary arteries:
 - Advanced modelling with device-specific material properties for BVS and patientspecific models for the stenosed coronary artery.
 - Coupling with Fluid Dynamics Module and Degradation Module, provides information regarding the drug-eluting BVS performance and efficacy in short term.



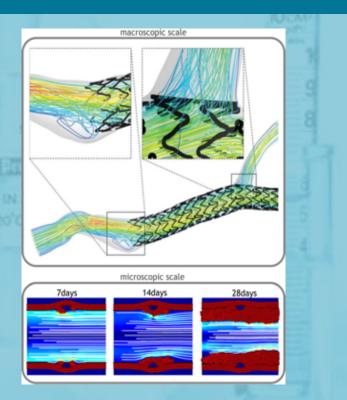


Fluid Dynamics Module





- Macroscopic scale: blood is treated as a continuum.
- **Microscopic scale:** multiscale models for describing the process of in stent restenosis.
- Blood components and vessel wall are included on a cellular level, and endothelial denudation, thrombus formation, SMC migration and the impact of the several laminae on the process of ISR is studied.

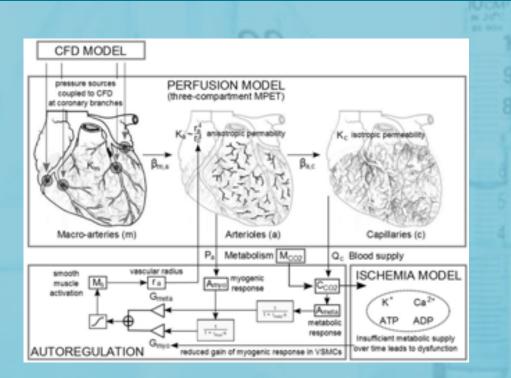




Myocardium perfusion Module



- A whole-heart myocardial perfusion model provides predictions of myocardial perfusion in the cardiac muscle.
- The Myocardial perfusion model is based on the "myocardium as a poroelastic medium" –with multiple overlapping compartments representing different scales of (micro)vasculature.





Drug-delivery Module



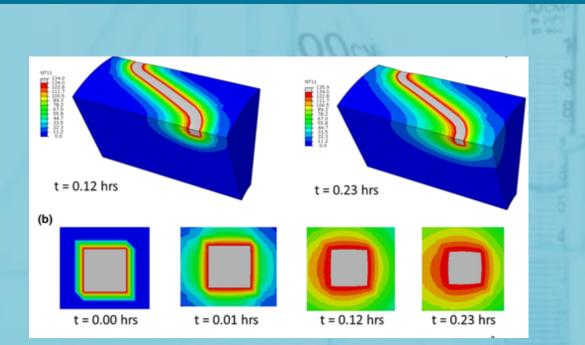
- The drug-delivery module includes 3D modelling of drug release employing most novel types of anti-proliferation drugs through:
 - flow-mediated convection of drug
 - transmural delivery of drug by plasma
 - effective diffusion inside the carrying polymer
 - porous tissue with anisotropic distribution of transport properties.
- Controlled transient release of drug from different layers of polymer include the phase change, diffusion and depletion.



Degradation Module



- Physico-chemical processes that are responsible for material degradation
- Multiphysics progression of degradation processes
- Models of the interaction of the degrading material with the surrounding environment

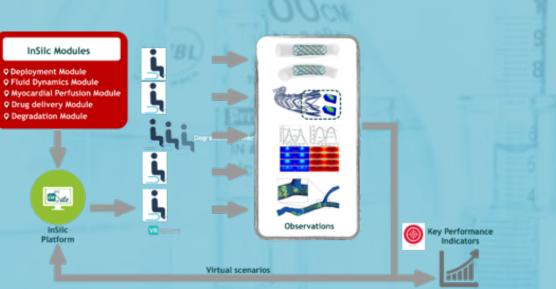




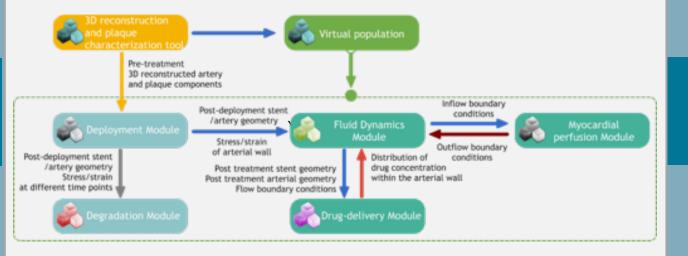
Virtual population



- "Virtual" patients to simulate the drugeluting BVS performance.
- "Virtual" scenarios include the alteration of the scaffold parameters to evaluate functional characteristics



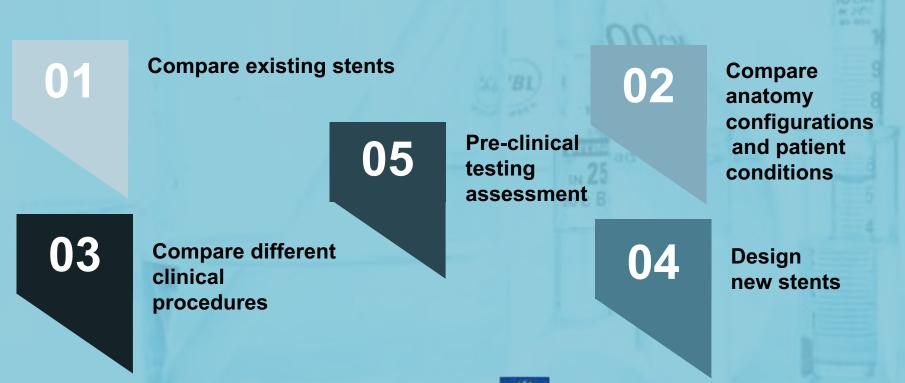




InSilc Scenarios

InSilc Scenarios







Virtual Population



- Virtual population is accessible as a database within InSilc platform.
- Each virtual patient's arterial geometries can be selected through a filtering tool.

	00
1	Arterial segment type
2	Presence of bifurcation
3	LDL and HDL values ranges
4	Comorbid condition Diabetes Hypertension Tachycardia
5	Degree and Length of Stenosis
6	Type of lesion



Virtual Population

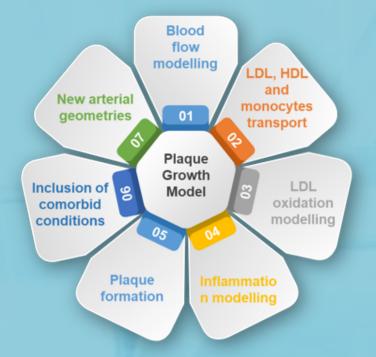


Dataset	- > Inputs	P rocess	C utputs	U sers
 Imaging data (IVUS, OCT, Angio, CT) Clinical data (risk factors, 	 3D reconstruction tool Arterial geometries (Retrospective data, prospective data) Boundary conditions Non-imaging data 	Plaque growth model Virtual arterial geometries	 Virtual patients with different characteristics (morphological and clinical) used by InSilc modules Stent Industry experts Contract Researce Organization Interventional Cardiologists Researchers 	experts • Contract Research Organization
biohumoral data)		Statistical model		Cardiologists
		Virtual patients combining geometries with clinical data		



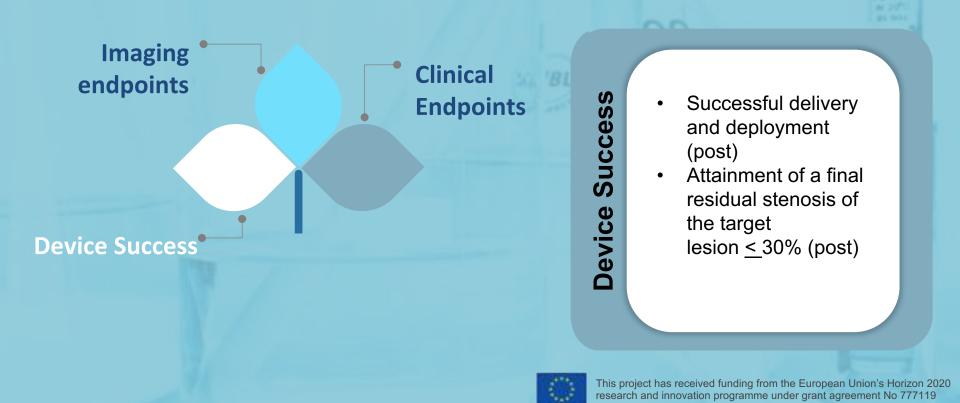
Plaque Growth Model Development

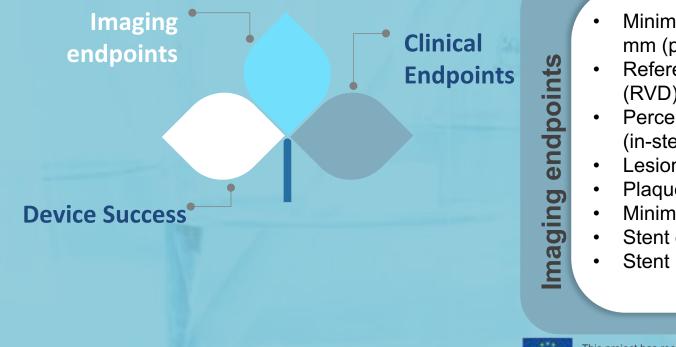




- Based on a previously developed model during SMARTool project.
- Simulation of main mechanisms of atherosclerosis.
- Utilisation of patient-specific data.
- Inclusion of comorbid conditions (diabetes, hypertension, tachycardia)
- Employment of FEA.
- Creation of new arterial geometries.

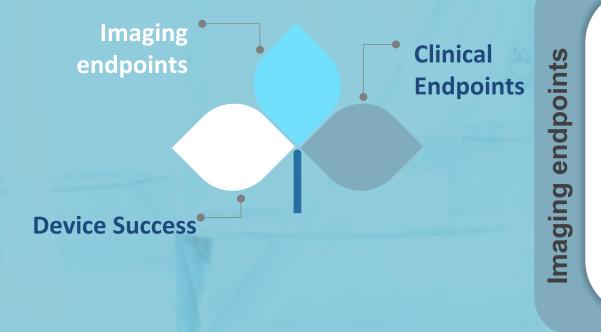






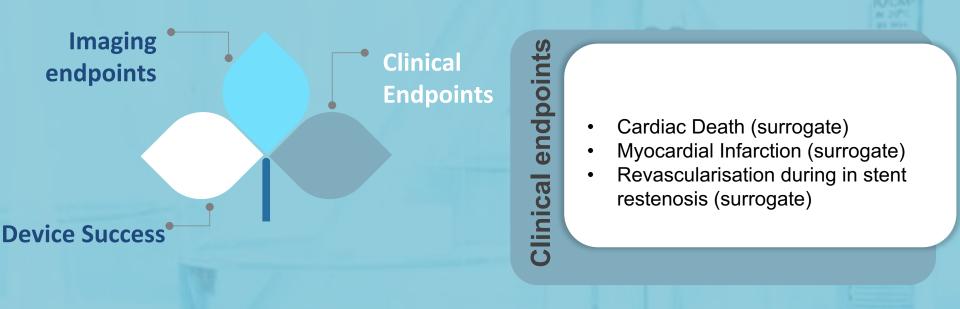
- Minimal lumen diameter (MLD) mm (pre)
- Reference vessel diameter (RVD) mm (pre, post, fu)
- Percentage diameter stenosis (in-stent/segment) (pre, post, fu)
- Lesion length (pre)
- Plaque burden (pre)
- Minimal stent area (MSA) (post)
- Stent expansion index (post)
- Stent underexpansion (post)





- Minimal lumen diameter (MLD) Post-procedural lumen eccentricity (post)
- Post-procedural lumen asymmetry (post)
- Malapposed stent struts (post)
- Stent edge dissection (post)
- Stent fracture (post)







InSilc Scenario 1 - Compare existing stents

- Polymer-based BVS performance may be different compared to permanent metallic DES.
- This scenario directly • compares behaviour Of both BVS DES and devices in the same artery and coronary provides clinically relevant insight into key features.

Related clinical trials			
Trial	Ν	Comparison	
Ellis et al. 2015	2008	Everolimus Eluting BVS vs Everolimus Eluting Stent	
Chevalier et al. 2015	501	Everolimus Eluting BVS vs Everolimus Eluting Stent	
Cassese et al. 2015	3738	Everolimus Eluting BVS vs Everolimus Eluting Stent	
Puricel et al. 2015	240	Everolimus BVS vs Everolimus or Biolimu s Eluting Stent	
Kereiakes et al. 2015	1684	Synergy vs Everolimus ES	
Byrne <i>et al.</i> 2019	262	Everolimus Eluting BVS vs Everolimus Eluting Stent	

[1] Ellis et al., N. Engl. J. Med., vol. 373, no. 20, pp. 1905– 1915, Nov. 2015.

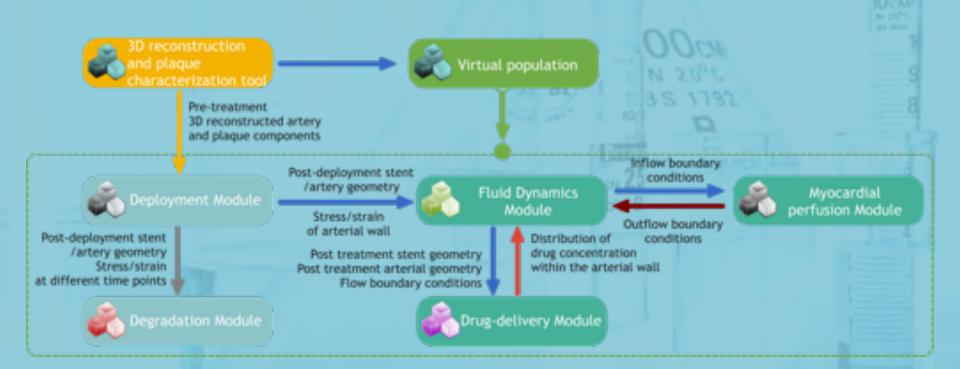
Chevalier et al., Eurointervention 2018;13: 1561-1564 [2] Cassese *et al., The Lancet*, vol. 387, no. 10018, pp. 537– 544, Feb. 2016. [3] Puricel et al., J. Am. Coll. Cardiol., vol. 65, no. 8, pp. 791–801, Mar. 2015.

Kereiakes *et al.*, *Circ. Cardiovasc. Interv.*, vol. 8, no. 4, Apr. 2015. [4] Byrne et al., European Heart Journal (2019)

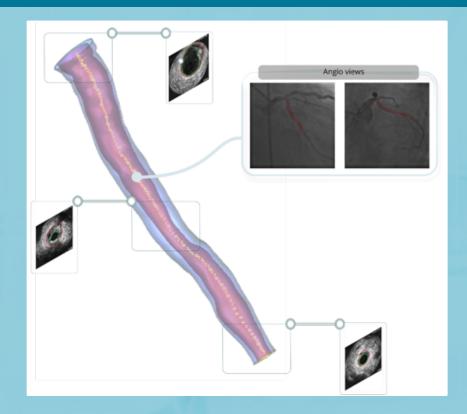
InSilc Scenario 1 - Compare existing stents In Silico approach

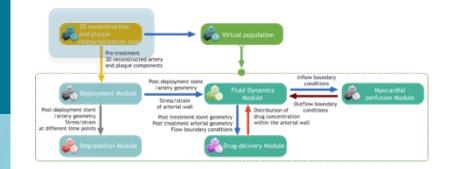
	Modules		Devices
3D reconstruction tool of coronary arteries and plaque characterization tool	Deployment Module	Fluid Dynamics Module	Absorb BVS Stent Single coronary artery with specific
Drug Delivery Module	Degradation Module	Myocardial Perfusion Module	Synergy Stent

In Silico approach

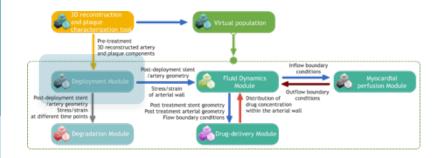


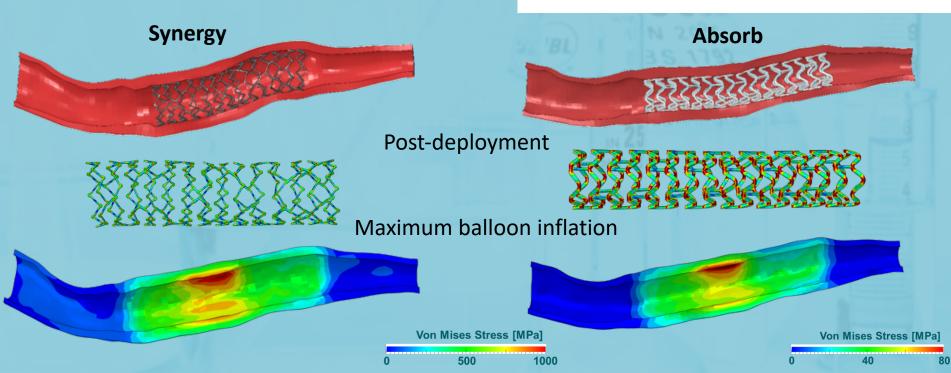


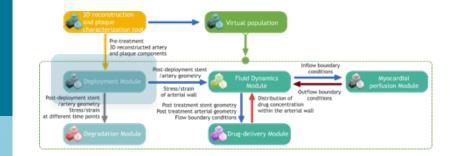




10 101) 1 N 20°C			
Vessel Characteristics			
Vessel length (mm)	44		
RVD (mm)	3.52		
Lesion length (mm)	17		
MLD (mm)	1.65		
Percentage diamet er stenosis	54%		

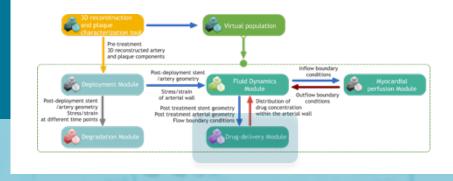






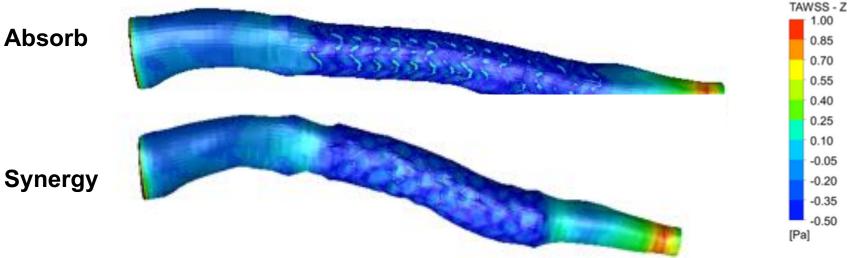
Short-term behaviour: post-deployment

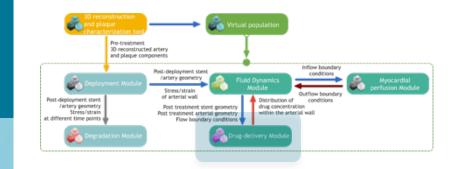
	Synergy	Absorb
Successful delivery and deployment	YES	YES
Final residual stenosis < 30% of the target	YES	YES
MLD - post-procedural [mm]	3.7	3.1
Diameter stenosis post-procedural [%]	0	12
Minimal stent area [mm2]	10.7	7.5
Stent expansion index [-]	1.10	0.77
Eccentricity index - EI [-]	0.96	0.96
Asymmetry index - AI [-]	0.08	0.09
Malapposed strut surface [%]	0	0
Stent edge dissection	NO	NO
Stent fracture	NO	NO



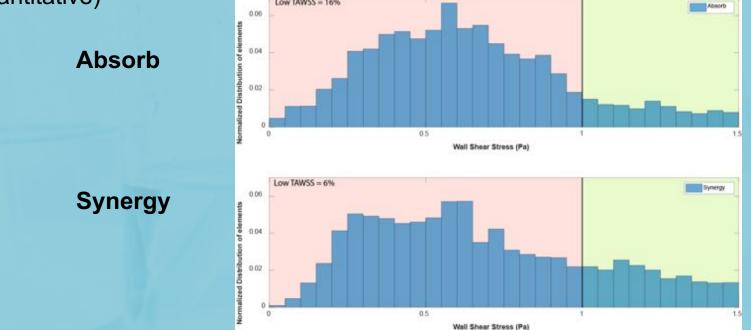
3D shear stress maps of the two stents (qualitative)



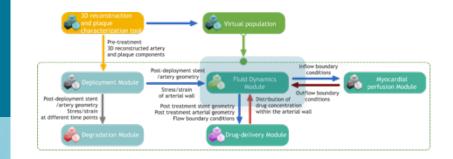


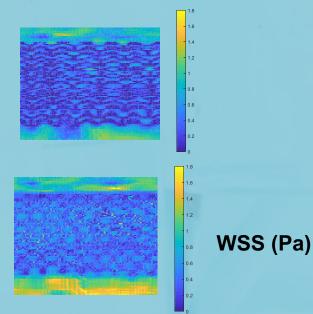


3D shear stress maps of the two stents (quantitative)

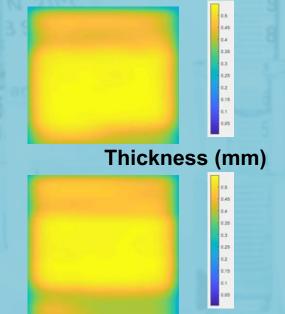


2D shear stress maps and predicted intima growth

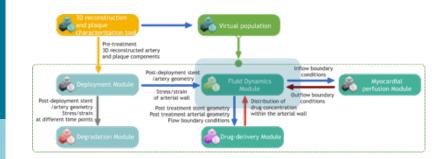




Fast responders 0.08 0.04 0.04 0.04 0.02 0.02 0.020.02



Thickness (mm)



Predicted imaging follow-up data

Absorb

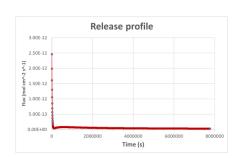
neo-intimal thickness MLA in-stent volume obstruction24% 0.41 mm 7.8 mm²

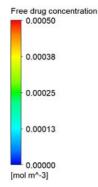
Synergy

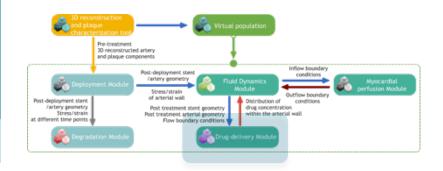
neo-intimal thickness MLA in-stent volume obstruction20% 0.4 mm 11.6 mm²

Free drug concentration at different times

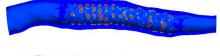
SYNERGY 1h 12h 24h 48h 72h

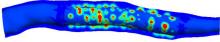


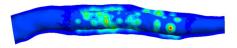


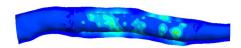


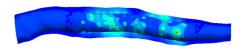
ABSORB

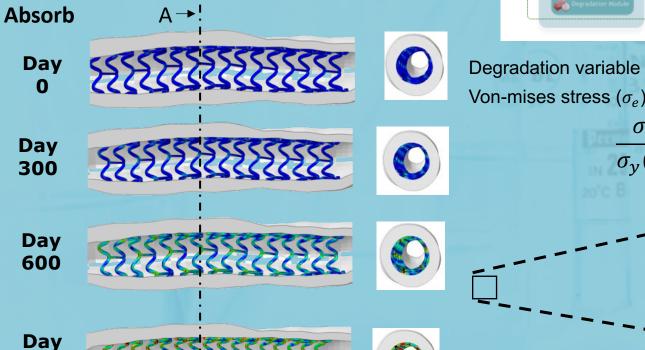


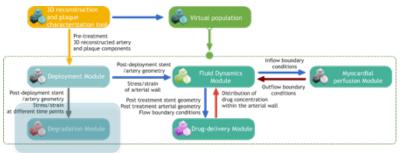












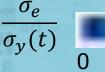
Degradation variable describes ratio of current Von-mises stress (σ_e) to current yield stress ($\sigma_v(t)$).

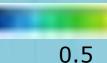


700

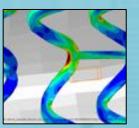
0



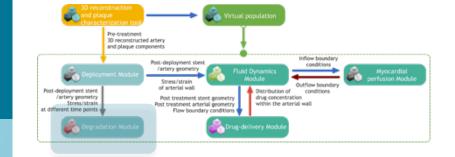




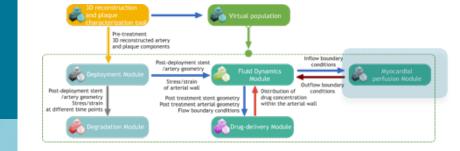


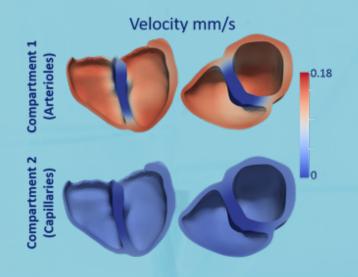


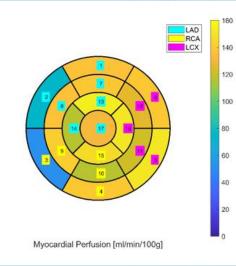
Damage due to degradation initiated ~Day 600



MODEL INPUT	Day 0	Day 300	Day 600	Day 700
Percentage diameter stenosis	n/a	n/a	n/a	n/a
Minimal stent area (MSA) (post)	Unchanged	Unchanged	98.4%	90.1%
Malapposed stent struts (post)	Unchanged	Unchanged	Unchanged	Unchanged
Stent fracture (post)	No	No	No (mild damage)	No (mild damage)
Late loss: in-stent and in-segment luminal loss (fu)	No	No	Minor	Minor
Strut discontinuity or dismantling	No	No	No	No



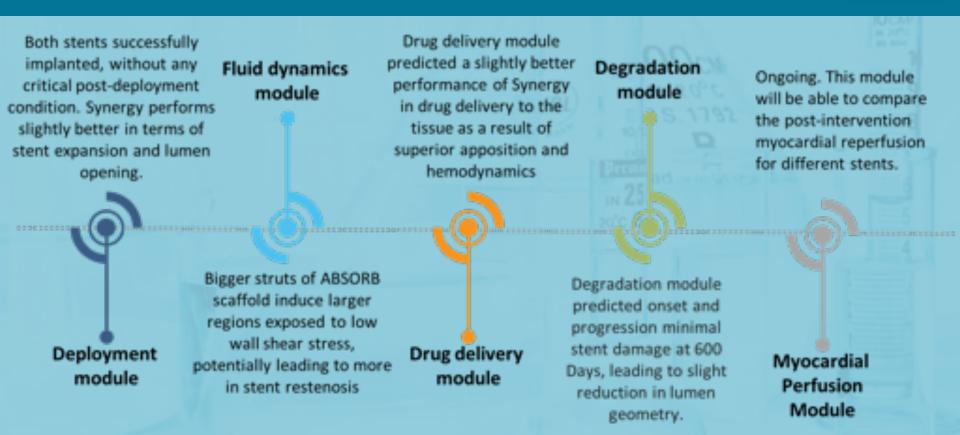




Myocardial perfusion [mL/min/100g] is used as surrogate to predict major adverse cardiac events (MACE)

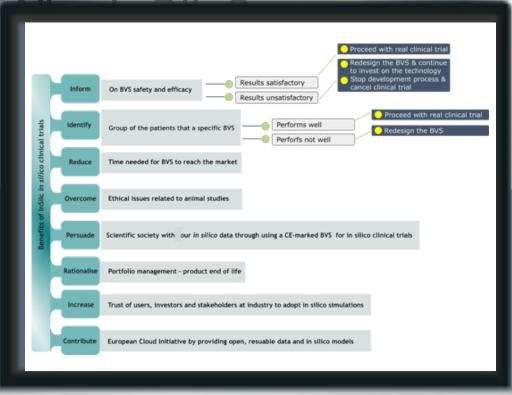
What did we learn?





Why in silico clinical trials?





_



- Identify the requirements for the certification of in silico trials for drug-eluting BVS
 - Provide evidence of the increase in the statistical power of InSilc by simulating more homogeneous and more «virtual» patients
 - Show the benefit in terms of clinical trials costs and duration
 - Estimate the reduction in animal testing
 - Define the target selection criteria of the patient population for reducing the need of complex and lengthy trials
- Study all regulatory issues which could prompt a transformation
 - Regeneration of the Stent Biomedical Industry to promote in silico trials
 - Explore the societal consequences of InSilc platform adoption
 - Investigate the standards to be taken into consideration
 - Define the ethical, privacy, secure data storage and management issues.





In silico clinical trial platform

Software as a medical device (SaMD) = software intended to be used for one or more medical purposes that perform these purposes without being part of a hardware medical device – Simulation as a medical device

for designing, developing and assessing

Intended use/ intended purpose = the objective intent of the manufacturer regarding the use of a product, process or service ...» Fundamental in the determination of its classification drug-eluting bioresorbable vascular scaffolds (BVS)

Class III medical device



This project has received funding from the European Union's Horizon 2020 research and innovation programme under grant agreement No 777119



Computational modeling can be part of a regulatory submission in two ways*:

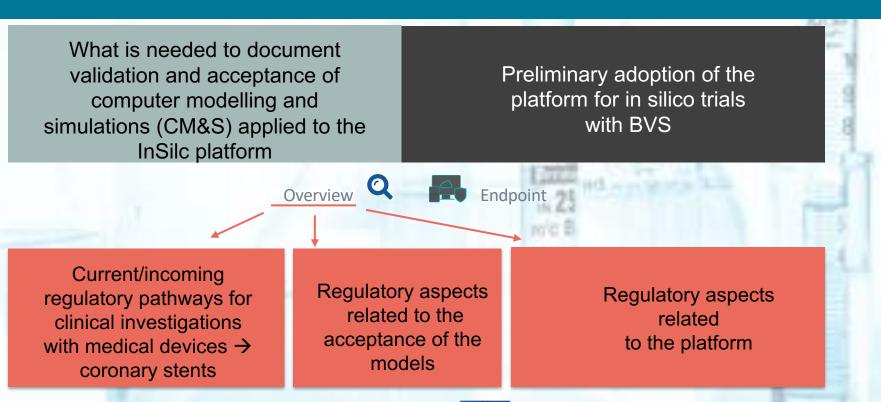
when simulation results serve as supporting (digital) evidence in a marketing application for a medical device when simulation is a medical device, such as for clinical decision support; this is "software as a medical device."

Simulation results to support the screening of new stents InSilc platform

Simulation results as supporting (digital) evidence: - mechanical testing - non-clinical testing: assessment of known risks by engineering failure modes Simulation results as supporting (digital) evidence

- "in silico" simulation of clinical trials based on standard surrogate endpoints









REGULATION (EU) 2017/745

Art 62 General requirements regarding clinical investigations conducted to demonstrate conformity of devices

Guidelines for the conduct of clinical trials with coronary stents

Report of an ECS-EAPCI Task Force on the evaluation and use of bioresorbable scaffolds

FDA - 2016 Guidance Reporting of Computational Modeling Studies in Medical Device Submissions

American Society of Mechanical Engineers (ASME) verification and validation (V&V) subcommittee on computational models of medical devices (ASME V&V 40 subcommittee)

Medical Device Innovation Consortium

FDA's Office of Science and Engineering Laboratories (OSEL)

IMDRF International Medical Device Regulation Forum

What we could conclude?



- Regulatory requirements and reference guidance for clinical investigations with BVS well established
- Regulatory guidelines for the acceptance of the models partially available, but adaptation to InSilc models is needed.
 - Main question for regulators: define the accepted level of accuracy and reproducibility
- Regulatory guidelines related to the platform as SaMD available

CRITICAL POINTS for the adoption of the platform for in-silico trials with BVS

- Clinical trial requirements for in silico trials are not existing
- Previous experience is missing
- The targeted clinical condition and the treatment have too many variables to be considered to allow for accurate and reliable simulations



Current regulatory activities



- Extensive collection and review of regulations, guidelines and publications
- Definition of the recognised short/mid-term surrogate endpoint to be tested in the modules
- Consulting with Prof. Viceconti (ex Insigneo Institute for *in silico* medicine Avice nna Alliance) and liaison with other in silico projects
- Consulting with invasive cardiologists members of ESC/EAPCI (ex task force on BVS)
- Contacts with European Forum for Good Clinical Practice
- Preliminary contacts with FDA and EMA



Future regulatory activities



- Work closely with:
 - Experts from the Medical Device Coordination Group and FDA
 - Notified Bodies
 - ISO experts
 - Avicenna Alliance
 - ESC/EAPCI
 - European Forum for Good Clinical Practice
 - EUCROF (European CRO Federation)

